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Advanced Opportunities in KAFO Fittings: SCO and SSCO

Thomas Schmalz, Heiko Drewitz

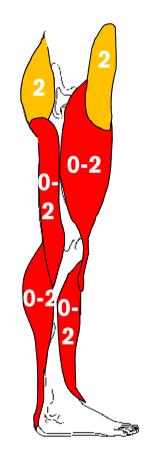


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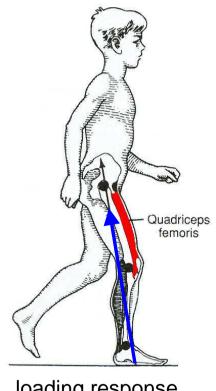
ottoboc Introduction

complex lower limb muscle weakness: **K**nee **A**nkle **F**oot **O**rthosis (KAFO)



impairment of patients' safety

(insufficient compensation of moments acting externally at knee and hip joint during ADLs)



loading response

functional task of orthosis: safety, highest possible functionality

Introduction ottobac

Knee Ankle Foot Orthosis (KAFO): Principles



principle A: free knee joint with posterior off-set



principle B: locked knee joint



principle C (SCO): knee joint locked (stance) and unlocked (swing)



principle D (SSCO):
MP controlled
stance and swing
(hydraulics)

- different level of safety
- restricted functionality (level walking)
- no knee flexion under weight bearing

- safety algorithm
- knee flexion under weight bearing
- swing phase control

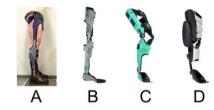
Introduction ottoboc

KAFO principles: functionality vs. safety functionality 1 ADLs with knee flexion under weight bearing level walking only "high" "low" safety



Introduction ottoboc

KAFO principles: evaluation of functionality and safety



- fitting experiences

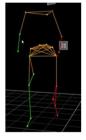






- scientific investigations: walking and standing
 - → biomechanical parameters
 - → metabolic parameters
 - specific safety parameters



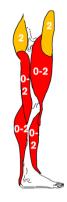






distinct knee extensor weakness: KAFO fitting

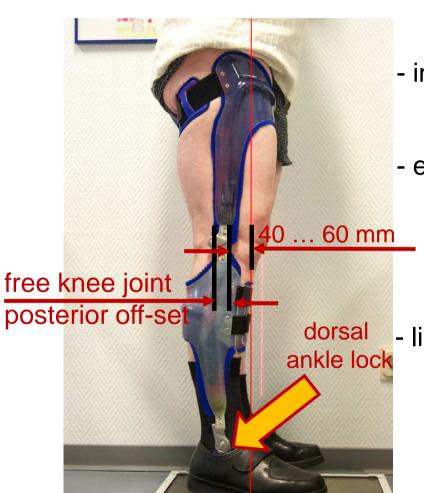




principle A: free knee joint / posterior off-set

Principle A ottoboc

principle A: free knee joint / posterior off-set



- individual KAFO (free joint / dorsal ankle lock)

- essential: alignment!

- limited safety level



functionality: walking on even ground

Principle A ottoboc

principle A: free knee joint / posterior off-set





distance load line – knee axis 20mm

insufficient!

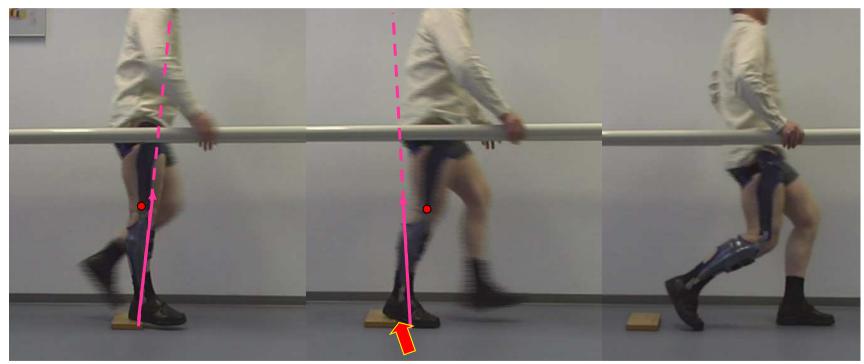
distance load line – knee axis 45mm

recommendation!

Principle A ottoboc

principle A: free knee joint / posterior off-set

walking on uneven ground: principle A insufficient



knee extension moment generated by GRF

knee flexion moment generated by GRF

risk of falling



distinct knee extensor weakness: KAFO fitting





principle B: completely locked knee joint

Principle B ottoboc

distinct knee extensor weakness: KAFO fitting principle B: completely locked knee joint





level walking:

- extremely safe

other ADLs:

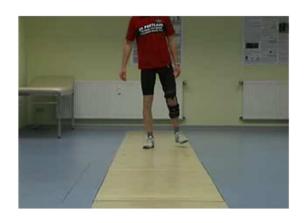
not possible (or extreme compensations)

Principle B ottoboc

completely locked knee: compensations (level walking)



increased frontal pelvic motion ("hip hiking")



2. circumduction

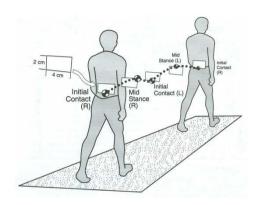


3. increased sound limb ankle joint motion ("vaulting")

(Perry 1992, Abdulhadi et al. 1996, Waters/Mulroy 1999, Irby et al. 2005)

Principle B ottoboc

completely locked knee: biomechanical consequences



normal:

medio-lateral motion: appr. 4cm

vertical motion: appr. 3 ... 5cm

1. vertical COM motion increased about 1.5cm





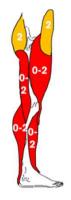
2. increased metabolic energy consumption: 18 ... 23% (Kerrigan et al. 1995)

distinct knee extensor weakness: KAFO fitting





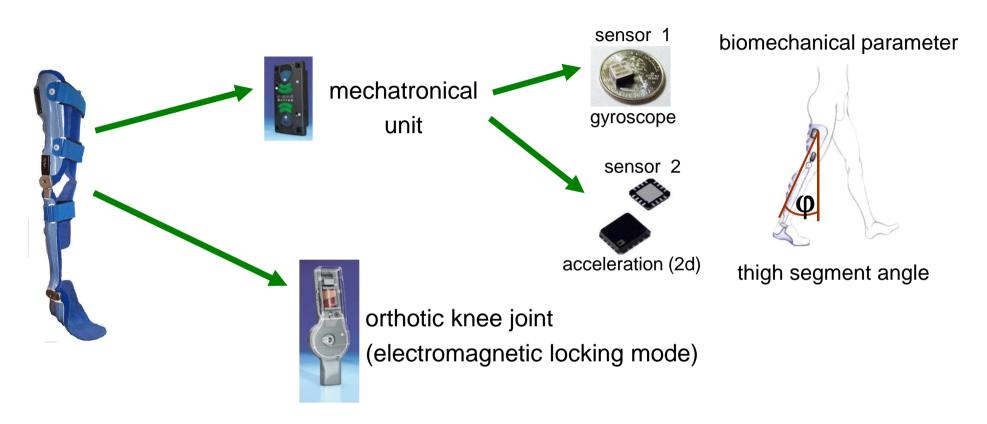




principle C (SCO): knee locked in stance, free in swing (partly with sensors)

Principle C ottoboc

principle C: E-MAG Active



- unlocking: knee extension moment and thigh segment angle threshold (50 .. 55% GC)
- locking: full knee extension (95% GC)
- both locked and unlocked mode ("SCO mode") can be tested



Principle C ottoboc

distinct knee extensor weakness: KAFO fitting

principle C: knee locked in stance, free in swing





level walking:

- improved gait pattern
- reduced level of safety

other ADLs:

 extreme compensations (non-physiological joint loading)

comparison: principle B vs principle C





- -biomechanical parameters
- -metabolic parameters

level walking

(n=8)



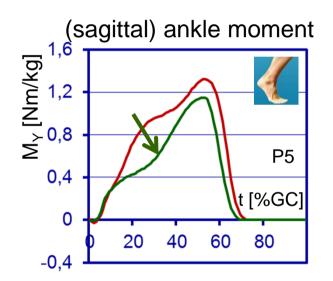
comparison: principle B vs principle C

compensatory mechanisms

hip hiking

- locked: measured for all

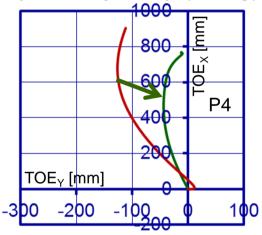
(sound side) vaulting



- locked: measured for 3/8
- reduced with SCO: 6/8 patients reduced with SCO (slightly for 2 patients)

circumduction

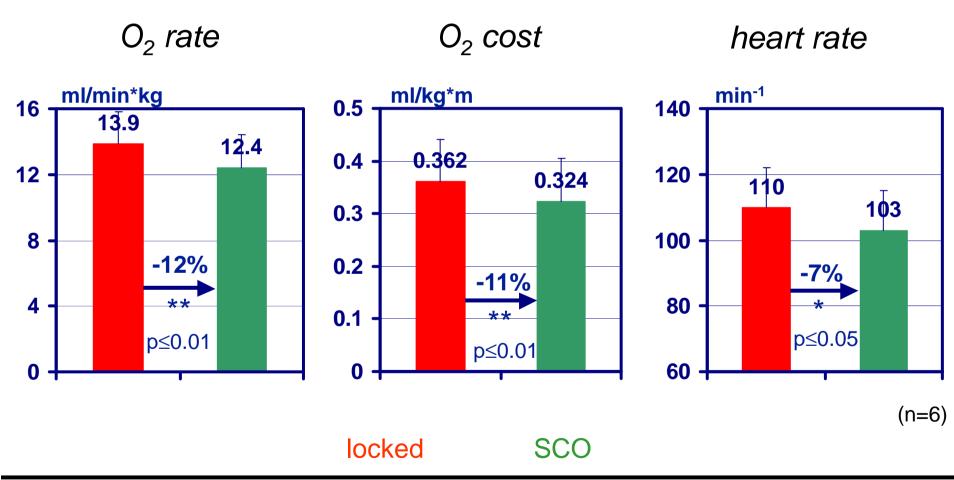
x,y toe trajectory (swing)



- locked: measured for 1/8
- reduced with SCO



comparison: principle B vs principle C metabolic parameters



comparison: principle B vs principle C

benefit resulting from principle C:

- 1. reduced metabolic energy consumption (10 15%)
- 2. reduced effort for initiation of swing phase
- 3. natural pelvic motion
- 4. reduced sound limb joint loading
- 5. significant clinical benefit
 - valid for level walking



distinct knee extensor weakness: KAFO fitting





principle D: SSCO microprocessor controlled stance and swing phase (hydraulic element)

principle D (SSCO)



microproccessor controlled KAFO:

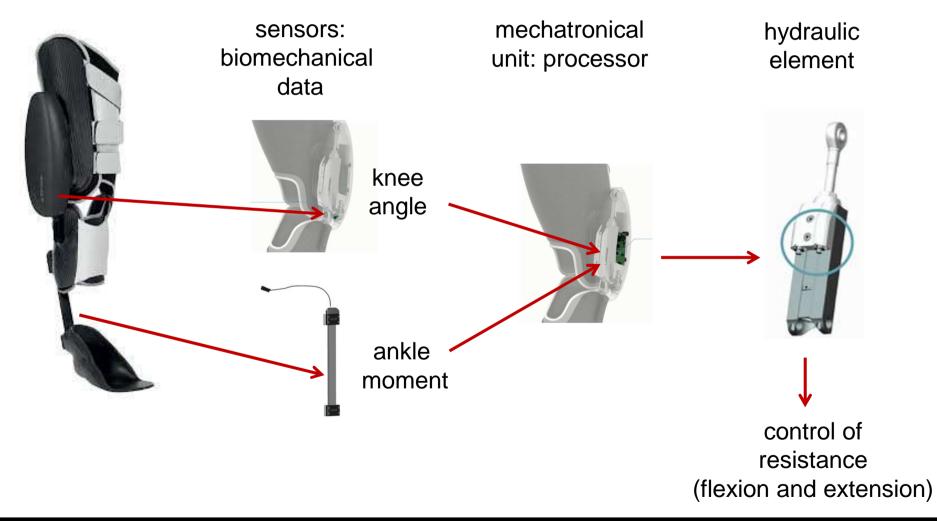
- individual control of stance and swing
- knee flexion under weight bearing (hydraulic element)



- difficult ADLs can be performed nearly natural
- high safety level

Principle D ottoboc

principle D (SSCO)



Principle D ottoboc

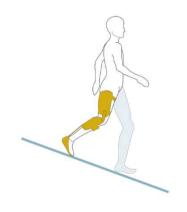
principle D (SSCO)

learning process: use of knee flexion under weight bearing





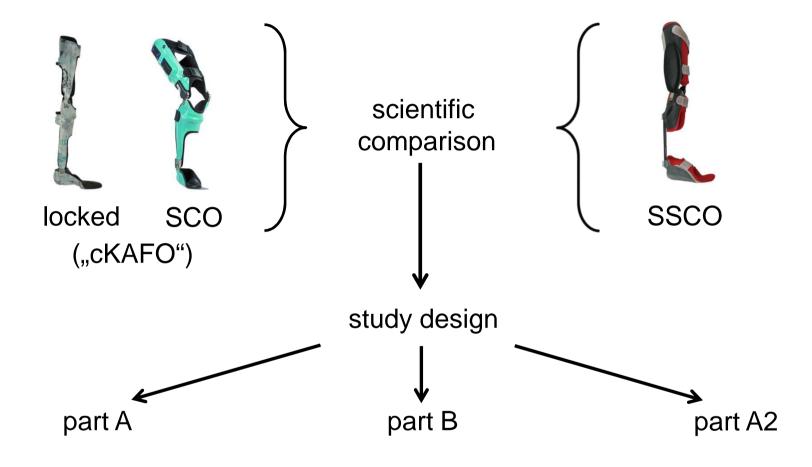












- biomechanical parameters
- different motions [Schmalz et al. 2014, 2016]

- metabolic parameters
- level walking

- test of safety
- level walking(even / uneven ground)





6 patients with cKAFOs: 4 SCO, 2 locked (3m / 3w; 32 ... 70y; 150 ... 176cm; 51 ... 89kg) biomechanical SSCO biomechanical metabolic test use of SSCO fitting (SSCO and test in daily live test (4 ... 6 weeks) (SSCO) (7 ... 30 weeks) cKAFO) (cKAFO) part B part A safety tests (SSCO and (4 ... 6 weeks) cKAFO) part A2



SSCO vs cKAFOs

biomechanical tests



level walking (3x at different v)



ramp (10°, descending)



stair (descending)

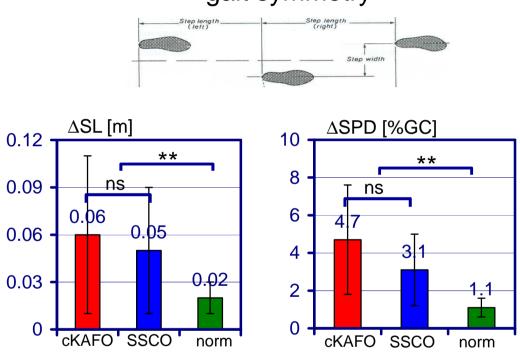


time - distance - parameters

walking speed

2 V [m/s] 1.5 ns 1.45 1.12 1.11 0.5 cKAFO SSCO norm

gait symmetry



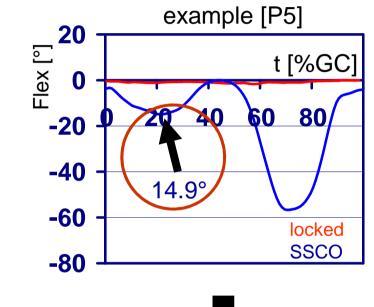
- patients: walking speed reduced, gait symmetry reduced
- no significant differences between SSCO and conventional KAFOs



stance phase flexion (Yielding)







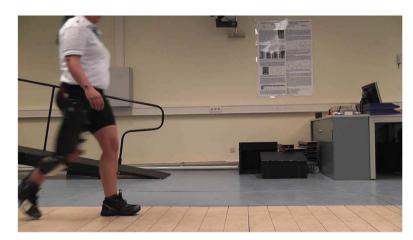


Yielding is used mostly:

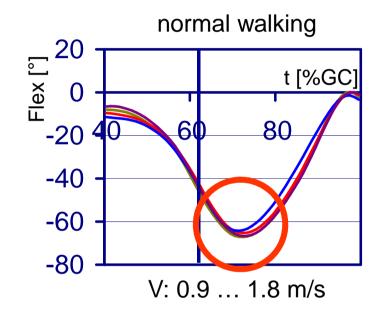
- 5 / 7 orthotic limbs (4 / 6 pat.)
- mean 11.0 ± 5.6°



swing phase control





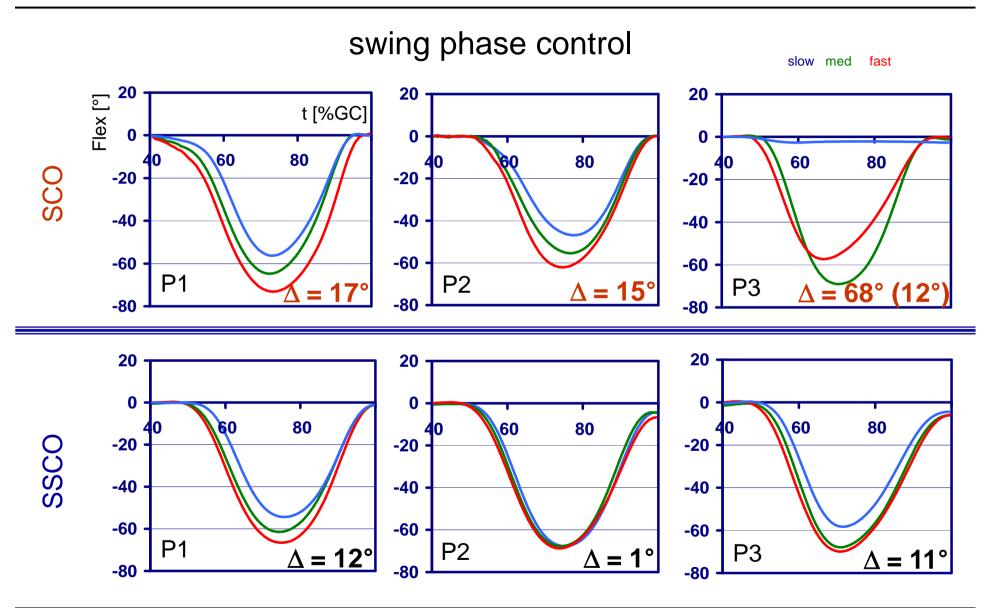


flexion: 63 ... 66°



nearly constant max swing phase flexion angle







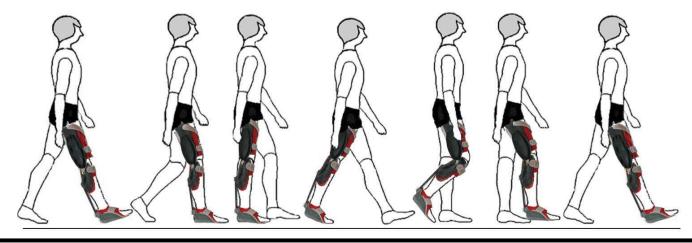


Level walking

- stance phase flexion is mostly used
- microprocessor controlled swing phase: easier speed variation, gait appears more natural

- joint loading: SSCO vs SCO: similar

SSCO vs locked KAFO: reduction

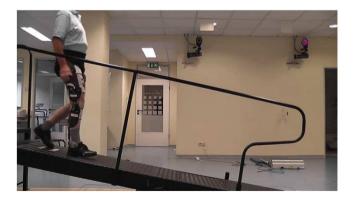




conventional KAFO: 4/6 with step-over-step pattern (hand rail: 4/4)



SSCO: 6/6 with step over step pattern (hand rail: 1/6)



conventional KAFO: 0/6 with step-over-step pattern



SSCO: 6/6 with step-over-step pattern (hand rail: 5/6)









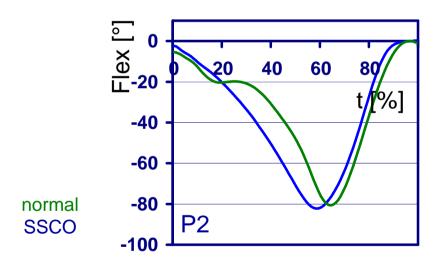


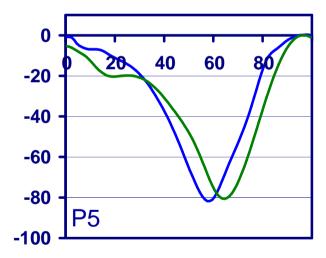






knee angle (orthotic limb)





continuous knee flexion under weight bearing in each case (independent from the previous fitting)



Descending ramps and stairs

- flexion under weight bearing with SSCO:
 - a) enables a nearly natural motion pattern
 - b) patients use this feature with a high degree of confidence
- SSCO vs. conventional KAFO: reduction of joint loading







Measurement of metabolic energy consumption







1 outdoor measurement(SCO: 3.0 km/h; SSCO: 3.6 km/h)



- 5 treadmill measurements (2.1 ... 3.0 km/h)

- data analysis: last minute of a 6 min test, randomized order, break: 30min.
- parameters of evaluation: oxygen rate, oxygen cost, heart rate



metabolic energy consumption: additional lower limb mass

cKAFO

SSCO



mass difference: 1 ... 1.5kg

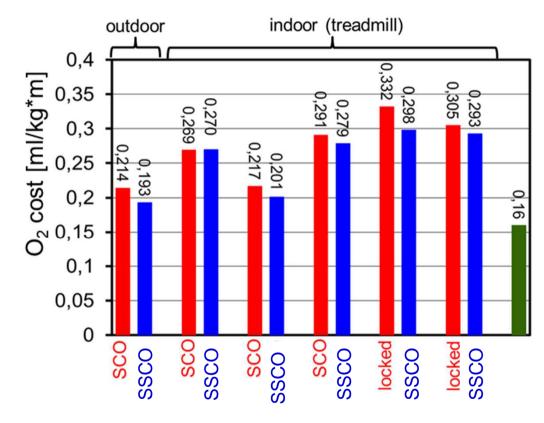


- additional mass lower limb mass (1 ... 2 kg):
 - increased energy consumption (5 10%) [Skinner et al. 1990, Browning et al. 2007]
- effect depends on location of additional mass [Schertzer & Riemer 2014]
- corresponding perceptions not reported by the patients

O₂ cost (independent of speed)



normal (mean)
locked KAFO /SCO
SSCO



- SSCO vs. cKAFO: -10% 0% -7% -4% -10% -4%

- statistics not useful (mixture of indoor/outdoor testing and locked KAFO/SCO)



- metabolic energy consumption: slightly decreased with SSCO possible reasons for compensation of "mass factor":
 - a) additional mass of SSCO located relatively proximal
 - b) use of SSCO functions with high degree of confidence





use of handrail: 1 / 6 patients

results indicate a considerably increased safety level of SSCO



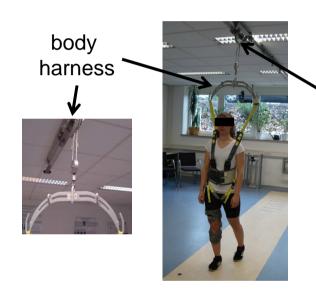
Testing of safety: protocol approved in prosthetics



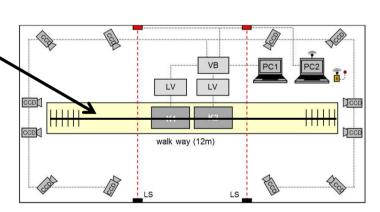
track (ceiling)

The Safety of C-Leg: Biomechanical Tests

Siegmar Blumentritt, PhD, Thomas Schmalz, PhD, Rolf Jarasch, CPO



measurement of biomechanical parameters (during level walking at self selected speed)



thin cord



test 1: step on an "obstacle"



test 2:
simulating of tripping
(disruption of swing extension)

test 1: step on an obstacle



SCO

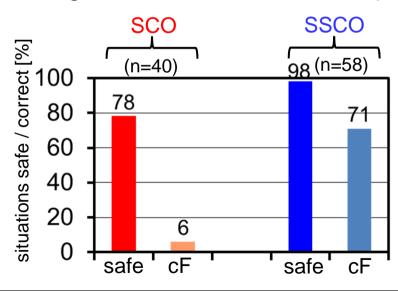
SSCO

fore foot contact



safe

risk of falling (unlocking condition reached too soon)



heel contact



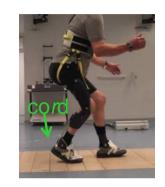
SCO

safe, but no correct function
(unlocking conditions not reached no unlocking procedure)

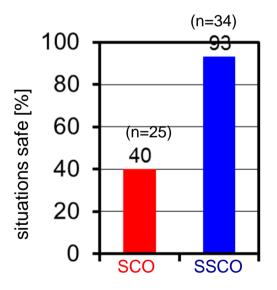


test 2: simulating of tripping (disruption of swing extension)

25 test trials with SCO



34 test trials with SSCO



- SSCO: only 2 /34 trials with risk of falling (when swing phase is disrupted near maximum flexion angle)
- damped flexion during weight bearing most important feature for fall prevention





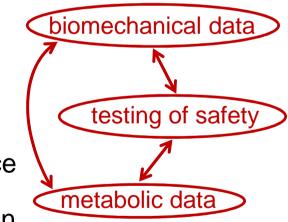
 SSCO principle expands range of ADLs with nearly physiological gait patterns

effects of loading reduction

- with SSCO considerably increased level of safety

→ slightly reduced metabolic energy consumption

- period of adaptation: 8 ... 12 weeks



KAFO principles: functionality vs. safety functionality 1 ADLs with knee flexion under weight bearing level walking only "high" "low" safety



Summary ottoboc













KAFO fitting: Which principle is suitable for a patient?

there is no universal assignment rule – patient might be fitted with all KAFO types

priority: evaluation of individual situation

- environmental conditions
- individual demands regarding activity and safety
- cosmetic aspects

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Thank you!